

Cartesian 3D-SHORE with Laplacian Regularization

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1 Introduction

The following is a description of the algorithm used to generate submissions to the Sparse Reconstruction Challenge for Diffusion MRI (SPARC dMRI) of the MICCAI 2014 Workshop on Computational Diffusion MRI. A total of three submissions were generated for the challenge #1 using the three-shells datasets with 20, 30, and 60 gradients per shells (b -values of 1000, 2000, and 3000 s/mm²). We pre-processed the data using a 3D Non-Local Means denoising [1] on each DWIs separately.

2 Method description

We used the 3D-SHORE Cartesian basis [2] with a Tikhonov regularization on the Laplacian to fit the dMRI signal. We solve the optimisation problem $\min_x \frac{1}{2} \|E - \Phi \cdot c\|_2^2 + \frac{\lambda}{2} \|R \cdot c\|_2^2$ where E is the normalized diffusion signal, Φ is the system matrix of size (number of q-points) \times (number of basis elements) (eq. 23 in [2]), c is the coefficient vector and R is the regularization matrix. We recast this optimization problem as a Quadratic Program and constrained the reconstructed signal at $\mathbf{q} = \mathbf{0}$ to be 1. We note that the present technique makes no attempt to promote sparsity on the coefficient vector.

For all datasets, we used $\lambda = 0.005$ and a maximal radial order (N_{max}) of 8 for the 30 and 60 gradients per shell datasets and 6 for the 20 gradients per shell dataset in the construction of Φ .

From the fitted coefficients c , we analytically compute the s^{th} order “radial moment” of the propagator $\int_0^\infty P(r\mathbf{u})r^{2+s}dr$ (eq. 33 in [2]). For example, Tuch’s diffusion ODF (dODF) corresponds to $s = -2$ and the classical dODF to $s = 0$. The ODFs are computed on a sphere of 5780 points with $s = 2$, promoting sharp angular profiles. The maxima extraction is performed discretely on min-max normalized ODFs and points with a relative amplitude ≥ 0.5 that are maximal inside a 25° neighbourhood are considered as true maxima.

The signal estimation is obtained by $E_{est} = \bar{\Phi} \cdot c$ where $\bar{\Phi}$ is a new system matrix computed from the desired q-points coordinates.

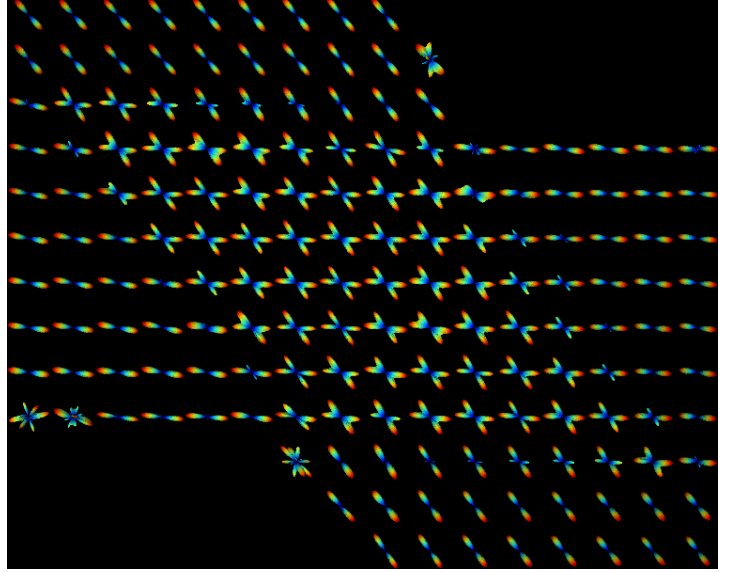


Figure 1: ODFs estimated from the 3-shells with 60 gradients directions per shell dataset.

References

- [1] Maxime Descoteaux, Nicolas Wiest-Daesslé, Sylvain Prima, Christian Barillot, and Rachid Deriche. Impact of rician adapted non-local means filtering on hardi. In *Medical Image Computing and Computer-Assisted Intervention (MICCAI)*, volume 5242, pages 122–130, 2008.
- [2] Evren Özarslan, Cheng Guan Koay, Timothy M. Shepherd, Michal E. Komlosh, M. Okan Irfanoglu, Carlo Pierpaoli, and Peter J. Basser. Mean apparent propagator (map) mri: A novel diffusion imaging method for mapping tissue microstructure. *NeuroImage*, 78(0):16–32, 2013.