

Deconvolution enhanced Generalized Q-Sampling 2 and DSI deconvolution

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For the purpose of the ISBI HARDI reconstruction challenge 2013 and for the heavyweight category, we reconstructed the diffusion datasets using two methods: a) Generalized Q-sampling Imaging 2 [1], [2] with spherical deconvolution [3],[4] (GQID), and b) Diffusion Spectrum Imaging with Deconvolution [5] (DSID).

GQI2 provides a direct analytical formula to calculate the solid angle ODF (ψ_{GQI2}) of DSI without the need to first estimate the diffusion propagator:

$$\psi_{GQI2}(\mathbf{u}) = \lambda^3 \int S(\mathbf{q})H(2\pi\lambda\mathbf{q} \cdot \mathbf{u})d\mathbf{q} \quad (1)$$

where \mathbf{u} is the unit direction in the sphere, \mathbf{q} is the q-space wave vector, S is the DW signal, λ is a smoothing parameter called the sampling length and

$$H(x) = \begin{cases} 2 \cos(x)/x^2 + (x^2 - 2) \sin(x)/x^3, & x \neq 0 \\ 1/3, & x = 0 \end{cases}$$

In [1], it was shown that ψ_{GQI2} creates ODFs with higher angular accuracy than standard DSI ODFs. In this work, we further extended ψ_{GQI2} with the spherical deconvolution transform (SDT).

The SDT is a sharpening operation which transforms the smooth diffusion ODF into a sharper fiber ODF [6]. The idea here is that an ODF for example the GQI2 ODF ψ_{GQI2} can be formed by convolution between the single fiber diffusion ODF kernel, R and the true fiber ODF ψ_{GQID}

$$\psi_{GQI2}(\mathbf{u}) = \int_{|w|=1} R(\mathbf{u} \cdot \mathbf{w})\psi_{GQID}(\mathbf{w})dw \quad (2)$$

The deconvolution is a fast converging iterative process.

In order to deal with the high levels of noise, the diffusion weighted (DW) datasets for SNR 10 and 20 were denoised with adapted non-local means filtering [7] using a rician noise model. As proposed in [7], each DW images were processed independently. The DW dataset with SNR 30 was left intact and no further denoising was performed.

In GQI2, we usually use $2 \leq \lambda \leq 3$ as higher values can give noisier ODFs as we see at Fig.1Left. However, higher values of λ have the advantage that we are sampling from a higher radius in q-space (higher b-values) where most of the angular information lives. Using the GQID, we show at Fig.1Right that we can eliminate those noisy peaks and obtain sharper ODFs.

Apart from the GQID, for comparisons we also performed reconstructions using DSI with deconvolution [5]. This deconvolution is not a spherical one, but it is performed in the 3D grid of the DSI propagator using Lucy-Richardson deconvolution. DSID is known to create very sharp ODFs from last year's ISBI challenge.

In order to find the best parameters for the methods described here, we created a connectivity matrix after generating deterministic streamlines from the ODFs of the training set using the method provided by [8]. We finally selected the parameters which minimized the number of missing and false bundles in the training set and used

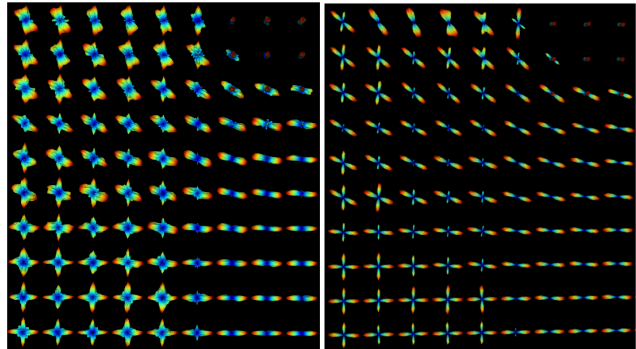


Fig. 1. A detail of slice Y=22 from the test data of the HARDI reconstruction challenge 2013 with GQI2 on the left and GQID ODFs on the right.

those with the test datasets. For DSID we used a propagator grid of $35 \times 35 \times 35$. For GQID we used sampling length of $\lambda = 3.5$, SDT ratio of 0.22 and spherical harmonic order of 8. For the challenge we submitted all results with ODFs saved as spherical harmonic coefficients of order 8. The source code for the methods described in this paper is available at dipy.org.

REFERENCES

- [1] E. Garyfallidis, *Towards an accurate brain tractography*. PhD thesis, University of Cambridge, 2012.
- [2] F. Yeh, V. Wedeen, and W. Tseng, "Generalized Q-sampling imaging," *IEEE Transactions on Medical Imaging*, vol. 29, no. 9, pp. 1626–1635, 2010.
- [3] M. Descoteaux, R. Deriche, T. R. Knösche, and A. Anwander, "Deterministic and probabilistic tractography based on complex fibre orientation distributions," *IEEE Transactions in Medical Imaging*, vol. 28, pp. 269–286, February 2009.
- [4] M. Descoteaux, *High Angular Resolution Diffusion MRI: from Local Estimation to Segmentation and Tractography*. PhD thesis, University of Nice-Sophia Antipolis, 2008.
- [5] E. J. Canales-Rodríguez, Y. Iturria-Medina, Y. Aleman-Gomez, and L. Melie-García, "Deconvolution in diffusion spectrum imaging," *NeuroImage*, vol. 50, no. 1, pp. 136–149, 2010.
- [6] J.-D. Tournier, F. Calamante, and A. Connelly, "Robust determination of the fibre orientation distribution in diffusion mri: Non-negativity constrained super-resolved spherical deconvolution," *NeuroImage*, vol. 35, no. 4, pp. 1459–1472, 2007.
- [7] M. Descoteaux, N. Wiest-Daesslé, S. Prima, C. Barillot, and R. Deriche, "Impact of rician adapted non-local means filtering on hardi," in *Medical Image Computing and Computer-Assisted Intervention (MICCAI)*, vol. 5242, pp. 122–130, 2008.
- [8] G. Girard and M. Descoteaux, "Anatomical tissue probability priors for tractography," in *International Conference on Medical Image Computing and Computer Assisted Intervention (MICCAI'12) - Computational Diffusion MRI Workshop*, pp. 174–185, 2012.